II. CLAIM AMENDMENTS

1-12. (Cancelled)

- 13. (Currently Amended) A neuro-ventilatory efficiency computation method for monitoring/controlling thea level of ventilatory assist produced by a ventilatory assistance system, comprising:
 - a) receiving a first signal representative of <u>a subject's</u> inspiratory effort—<u>and</u>; the first signal having a first amplitude;
 - b) receiving a second signal representative of a lung volume and of the subject, the second signal having a second amplitude;
 - c) calculating a <u>neuro-ventilatory efficiency representative</u>

 <u>parameter in relation to between</u> said first and second amplitudes at predetermined intervals; and
 - d) increasing or decreasing the ventilatory assist level depending on whether a present calculated value of said relation the neuro-ventilatory efficiency representative parameter is higher or lower than a past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding a given threshold.
 - 14. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, wherein said relation calculating a neuro-ventilatory efficiency representative

parameter comprises calculating a ratio between said first and second amplitudes at predetermined time intervals.

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- 15. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, wherein said relation calculating a neuro-ventilatory efficiency representative parameter comprises calculating a ratio between said first and second amplitudes at intervals when one of said first and second amplitudes reaches a predetermined level.
- 16. (Currently Amended) Α neuro-ventilatory efficiency computation method as in claim 13, wherein increasing or decreasing the ventilatory assist level increasing or decreasing comprises increasing the ventilatory assist level when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is higher than said past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding the threshold, and decreasing the ventilatory assist level when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is lower than said past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding said threshold.
- 17. (Previously Presented) A neuro-ventilatory efficiency computation method as in claim 13, wherein receiving the second signal representative of a lung volume comprises receiving a signal representative of a given lung volume.

- 18. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, wherein receiving the first signal representative of the subject's inspiratory effort comprises receiving a signal representative of a given level of inspiratory effort.
- 19. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, further comprising generating an alarm signal when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is higher or lower than the past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding said given threshold.
- 20. (Previously Presented) A neuro-ventilatory efficiency computation method as in claim 13, comprising manually performing said increasing or decreasing of the ventilatory assist level.
- 21. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, comprising expressing the first signal representative of the subject's inspiratory effort as one of the following values: a mean of said first amplitude, a median of said first amplitude, and a peak of said first amplitude.
- 22. (Previously Presented) A neuro-ventilatory efficiency computation method as in claim 13, comprising expressing the second signal representative of a lung volume as one of the

following values: a mean of said second amplitude, a median of said second amplitude, and a peak of said second amplitude.

- 23. (Currently Amended) A neuro-ventilatory efficiency computation method as in claim 13, wherein receiving the first signal representative of inspiratory effort comprises receiving an electromyographic signal from at least one muscle of a patient be subject.
- 24. (Currently Amended) A neuro-ventilatory efficiency computation device for monitoring/controlling thea level of ventilatory assist produced by a ventilatory assistance system, comprising:
 - a) a first input for receiving a first signal representative of a subject's inspiratory effort—and; the first signal having a first amplitude;
 - b) a second input for receiving a second signal representative of a lung volume and of the subject, the second signal having a second amplitude;
 - c) means for calculating a calculator of a neuro-ventilatory efficiency representative parameter in relation between to said first and second amplitudes at predetermined intervals; and
 - d) means for increasing or decreasing the ventilatory assist

 level depending control dependent on whether a present

 calculated value of said relation neuro-ventilatory

 efficiency representative parameter is higher or lower than

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a past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding a given threshold to increase or decrease the ventilator assist level.

25. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, wherein:

the <u>ealculating means</u> <u>calculator</u> comprises a divider responsive to the first and second amplitudes for calculating a ratio between said first and second amplitudes at predetermined intervals;

the increasing or decreasing means control comprises:

- a comparator responsive to the present calculated value and calculated value of said relationneuropast for ventilatory efficiency representative parameter producing a signal representative of a comparison between calculated value of said relationneuropresent ventilatory efficiency representative parameter and a past relationneuro-ventilatory calculated value of said efficiency representative parameter;
- an adder interposed between the comparator and the ventilatory assistance system for adding a preset increment to or subtracting a preset decrement from said ventilatory assist level when the comparison signal exceeds a given threshold.

- 26. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, wherein said ealculating meanscalculator comprises means for calculating said relationneuro-ventilatory efficiency representative parameter at predetermined time intervals.
- 27. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, wherein said calculating means calculator comprises means for calculating said relationneuro-ventilatory efficiency representative parameter at intervals when one of said first and second amplitudes reach a predetermined level.
- 28. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 25, wherein said adder comprises means for adding said preset increment to said ventilatory assist level when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is higher than said past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding said given threshold, and means for subtracting said preset decrement from said ventilatory assist level when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is lower than said past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding said given threshold.
- 29. (Previously Presented) A neuro-ventilatory efficiency computation device as in claim 24, wherein the second signal

representative of a lung volume is a signal representative of a given lung volume.

- 30. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, wherein the second first signal representative of the subject's inspiratory effort is a signal representative of a given level of inspiratory effort.
- 31. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, further comprising an alarm generator to produce an alarm signal when said present calculated value of said relationneuro-ventilatory efficiency representative parameter is higher or lower than the past calculated value of said relationneuro-ventilatory efficiency representative parameter by an amount exceeding said given threshold.
- 32. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 2425, wherein said adder comprises a manual adjustment system to add said preset increment to or subtracting said preset decrement from said ventilatory assist level.
- 33. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 2224, comprising means for expressing the first signal representative of the subject's inspiratory effort by means of one of the following values: a mean of said first amplitude, a median of said first amplitude, and a peak of said first amplitude.

- 34. (Previously Presented) A neuro-ventilatory efficiency computation device as in claim 24, further comprising means for expressing the second signal representative of a lung volume by means of one of the following values: a mean of said second amplitude, a median of said second amplitude, and a peak of said second amplitude.
- 35. (Currently Amended) A neuro-ventilatory efficiency computation device as in claim 24, wherein the first signal representative of the subject's inspiratory effort is an electromyographic signal from at least one muscle of a patient the subject.